

Research Article

Reduced Blood to Brain Glucose Transport as The Cause For Hyperglycemia: a Model That Resolves Multiple Anomalies in Type 2 Diabetes

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Classically, type 2 diabetes is believed to be a result of insulin resistance and relative insulin deficiency. However, evidence has been accumulating against the insulin resistance models. Absence of lasting hyperglycemia by insulin receptor knockouts or insulin suppression, evidence for hyperinsulinemia preceding insulin resistance, the perplexing hyperinsulinemic normoglycemic state, reduced glucose transport to the brain preceding hyperglycemia, signs of vasculopathy preceding hyperglycemia, absent or poor correlation between fasting glucose and insulin, very strong positive correlation between indices of insulin resistance and β cell function in population data are some of the anomalous findings which classical glucose homeostasis models have not addressed so far. With increasing evidence for neuronal involvement in glucose regulation, we propose a refined model of glucose regulation that considers brain glucose and insulin levels as the ultimate target of homeostasis and combines central and peripheral mechanisms of regulation. A model considering the reduced rate of blood-to-brain transportation of glucose and insulin as primary pathology explains most of the patterns, with or without insulin resistance. Apart from resolving multiple anomalies, the model also accounts for the failure of glucose normalization in effectively reducing diabetic complications and mortality.

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1. Introduction

Presently, any metabolic disorder with consistently raised plasma glucose and insulin resistance, which cannot be categorized into either type 1 diabetes or gestational diabetes, is defined as type 2 diabetes mellitus (T2DM) (DeFronzo et al., 2015). It is the most common form of diabetes, accounting for over 90% of all cases. The classically perceived cause of hyperglycemia in T2DM is insulin resistance followed by failure of compensatory insulin response. Historically, the role of the brain in glucose homeostasis was revealed by experiments in which damage to the fourth cerebral ventricle was shown to impair homeostatic control (Bernard, 1859). However, at a later stage, pancreatic extracts were shown to lower glucose and eventually, insulin was identified as the active principle (Banting et al., 1922). It is necessary to note that the differentiation of type 1 and type 2 diabetes was not made at that time. The success of insulin was so spectacular that all other mechanisms of glucose regulation were almost forgotten (Lundqvist et al., 2019). The distinction between type 1 and type 2 diabetes was to become clear half a century later, and it was realized that, unlike in type 1, insulin deficiency was not the primary cause of hyperglycemia in type 2 diabetes. However, by this time, the thinking in the field was so much insulin-centred that the inability of normal or increased levels of insulin to regulate plasma glucose was termed insulin resistance without carefully evaluating alternative hypotheses.

Further, the insulin resistance hypothesis is criticized for having a circular logic, which makes it unfalsifiable (Diwekar-Joshi & Wheatve, 2020). Insulin resistance is said to be responsible for the inability of normal or raised levels of insulin to regulate glucose. However, insulin resistance itself is measured by the inability of insulin to regulate glucose. There is no independent measure of insulin resistance that can be used to test the causal role of insulin resistance. Impairment of insulin signalling or fasting insulin levels in experiments using (i) tissue-specific insulin receptor knockouts (Blüher et al., 2002; Kadowaki, 2000) (ii) insulin-degrading enzyme knockouts (Costes & Butler, 2014; Maianti et al., 2014) (iii) pharmaceutical insulin suppression by diazoxide and octreotide (Giustina et al., 1991; Lamberts & Hofland, 2019; Leahy et al., 1994; Matsuda et al., 2002) (iv) insulin gene suppression by RNAi (Mehran et al., 2012b) (v) alteration in insulin gene dosage (Templeman et al., 2015) failed to alter fasting glucose in the expected direction. In epidemiological data, fasting insulin and fasting glucose are poorly correlated, while post-meal insulin and glucose are strongly correlated, unlike what would be expected by any of the classical models. With converging multiple lines of evidence, Diwekar-Joshi and Watve (2020) raised doubts about whether insulin resistance and failure of compensatory hyperinsulinemia is a necessary and sufficient explanation of fasting hyperglycemia.

Many mathematical models have been constructed based on the assumption of insulin resistance. A common set of assumptions is shared by most of the models that fasting glucose is the steady state achieved by a balance between glucose uptake by tissues and glucose production by the liver. One of the foundational assumptions is that both the above processes are regulated by insulin signalling in the steady state (Matthews et al., 1985). Therefore, insulin signalling has been central to these models. Since recent research has exposed the inadequacies of this model (Diwekar-Joshi & Watve, 2020), there is a need to hunt for better alternative models.

An alternative to the classical model, which assumes brain glucose level as the target of homeostasis, has been suggested, and mathematical models incorporating this concept have been constructed (Gaohua & Kimura, 2009; Watve, 2013). These models have not been explored sufficiently towards a comparative evaluation with peripheral models with respect to their predictions and their physiological as well as clinical implications. Here, we refine the brain-centred model further, incorporating recent evidence, evaluate its performance in explaining the accumulated anomalies and explore its physiological and clinical implications.

1.1. What a glucose homeostasis model needs to explain

Most models of glucose homeostasis have a limited goal of explaining altered fasting steady-state glucose levels and the alterations in the glucose curve in the prediabetic and diabetic states. However, now we have a large number of experimental results that are potentially anomalous. A model prediction matrix, in which each model is tested for matching its prediction with multiple known empirical patterns, is an appropriate and robust approach to comparing alternative models. Such an approach has been used to test alternative hypotheses in a number of other contexts (Shinde et al., 2021; Thakar et al., 2003; Vibishan & Watve, 2020; Watve & Diwekar-Joshi, 2016), and it can be the right approach to test alternative models of glucose homeostasis in T2DM. A model of choice would be one which can predict all or most of the known physiological patterns in type 2 diabetes so that no or minimal anomalies are left. We take a few steps towards a model prediction matrix, although a lot more exploration of many other models is required before constructing such a matrix.

Following is the list of known empirical patterns that a model needs to be compatible with.

1. The model should allow stable, steady state glucose on fasting: Fasting glucose is assumed to be a steady state with adequate evidence (Lerner & Porte, 1972; Matthews et al., 1985; R. C. Turner et al., 1979). Achieving a steady state is one of the primary objectives of every homeostasis model. Many of

the key concepts of classical models are also based on achieving a steady state in the fasting condition (Matthews et al., 1985; R. C. Turner et al., 1979).

2. The model should also allow stable, steady-state insulin on fasting. Normally, this is not a problem for any model; however, many models have a problem explaining the altered steady-state insulin level in a prediabetic state, as explained below.
3. Prediabetic state of normoglycemia with hyperinsulinemia: A prediabetic state is often accompanied by a high level of fasting insulin (*FI*) but normal fasting glucose (*FG*) in the plasma. This is not easy to achieve in a model. The classical qualitative explanation of this state is that it is a state of insulin resistance with a compensatory rise in *FI* such that *FG* remains normal. For this to happen, there is a need to estimate the level of insulin resistance and regulate insulin secretion accordingly. It is possible to hypothesize a mechanism for sensing insulin resistance and conveying this information to the pancreas. Such a mechanism can be glucose-dependent or glucose-independent. Currently, no glucose-independent mechanism for accurately assessing insulin resistance and conveying it to β cells is known. A common assumption is that insulin resistance reduces glucose uptake, thereby increasing *FG*. The rise in *FG* stimulates insulin production, and the rise in insulin levels normalizes glucose again. However, this mechanism fails to achieve a steady state of hyperinsulinemic normoglycemic condition (Diwekar-Joshi & Watve, 2020). Plasma insulin has a short half-life, and after glucose levels are normalized, it is unlikely to stay at a higher level unless there is a glucose-independent trigger for insulin secretion. Explaining a hyperinsulinemic normoglycemic steady state is a tricky challenge that any model needs to meet.
4. Hyperinsulinemia precedes insulin resistance and T2DM: Although hyperinsulinemia is believed to be a compensatory response to insulin resistance, a number of studies show that hyperinsulinemia precedes obesity and insulin resistance (Corkey & Shirihai, 2012; Mehran et al., 2012a; Pories & Dohm, 2020; Shanik et al., 2008; Weyer et al., 2000; Wiebe et al., 2021). This raises two independent questions. One is how and why hyperinsulinemia precedes insulin resistance. The second, more perplexing question is that if hyperinsulinemia is not a compensatory response to insulin resistance, the failure of compensation explanation becomes redundant. This needs to be replaced by a more coherent explanation of hyperglycemia.
5. The model should explain the following features of the post-meal glucose curve and its alterations in prediabetic and diabetic states, which cumulatively are called impaired glucose tolerance curves.
 1. Increased height of peaks
 2. Delayed return to normal

3. An increase in the time difference in glucose and insulin peaks in the diabetic state.
6. The normal fasting glucose with impaired glucose tolerance (NFG-IGT) state: It is common to find that in a prediabetic state, the glucose tolerance curve is altered with a normal level of fasting glucose.
7. Stress hyperglycemia: Why and how stress causes hyperglycemia only in some individuals (Dungan et al., 2009) needs to be explained by a model with realistic and testable assumptions.
8. Hyperglycemia after intensive exercise: If in a fasting state, *FG* is a result of the rate of liver glucose production and glucose disposal, an exercise that increases glucose disposal should decrease *FG*. However, in some studies, plasma glucose remains unchanged or is increased after exercise (Coggan, 1991; Marliss & Vranic, 2002). A model needs to predict this result contextually.
9. An important challenge is to explain why insulin receptor knockouts specific to muscle, fat cells or the liver result in normal fasting glucose but altered post-glucose load curves. Similarly, insulin-degrading enzyme knockouts do not alter *FG*. Also, insulin suppression by agents such as octreotide or diazoxide fails to alter *FG* (Diwekar-Joshi & Watve, 2020). A model should explain these observations. Diwekar-Joshi and Watve (2020) further differentiated between the consequential steady state (CSS) and targeted steady state (TSS) models and demonstrated that the results of the insulin receptor knockout and insulin suppression experiments can be explained by a TSS but not by a CSS model. In effect, to be able to account for these results, a model needs to be a TSS model.
10. Reduced glucose transport to the brain, particularly in obese or prediabetic individuals: It has been known over a long time that in type 2 diabetes, the rate of glucose transport from blood to the brain is slowed down substantially (Gjedde & Crone, 1981). In rodent models, the *glut-1* expression in brain capillaries is shown to be reduced (Cornford et al., 1995; Matthews et al., 1985; Pardridge et al., 1990). This has been viewed as a response to hyperglycemia. However, Hwang et al. (2017) show that subnormal transport is evident in obese and presumably prediabetic states, even before hyperglycemia appears. A model needs to account for this pattern as a causal or consequential phenomenon.
11. The T2DM-specific islet amyloid deposition, which often accompanies islet deterioration: Islet amyloid deposition is frequently associated with type 2 diabetes but not observed in type 1. The causes of islet amyloid deposition should be compatible with the glucose homeostasis model (Höppener et al., 1999; Porte & Kahn, 1989; Watve, 2014).
12. B cell deterioration pattern: The deterioration of β cells appears to follow a peculiar pattern in T2DM, in which a substantial proportion of β cells survive lifelong (Bacha et al., 2013; Butler et al., 2003;

Clark et al., 2001; Porte & Kahn, 2001; Watve, 2014). If dysfunction and damage to the β cell population are assumed to be an essential prerequisite of hyperglycemia in a model, the models need to account for the peculiar population dynamics of β cells.

13. Increased liver glucose production as well as ketogenesis with SGLT2 inhibitors: Over the last decade, SGLT2 inhibitors, which allow greater clearance of glucose through urine, have offered a novel means of combating hyperglycemia. Lowering of plasma glucose by SGLT2 inhibitors is accompanied by increased liver glucose production as well as increased ketogenesis (Limenta et al., 2019; Mistry & Eschler, 2021; Op den Kamp et al., 2021; Pfützner et al., 2017) The causes of which should be made clear by the model.
14. The Somogyi phenomenon, i.e., hyperglycemia following infusion of insulin, is seen in at least some cases of T2DM but not in healthy individuals. This can happen without being overtly hypoglycemic (Campbell, 1976; Reyhanoglu & Rehman, 2021).
15. In cases of brain injury, hyperglycemia is common (Shi et al., 2016). In bacterial meningitis, hyperglycemia is often observed, accompanied by low CSF glucose levels (Krishnan et al., 2016; Schut et al., 2009). A model should be able to account for the apparent contradiction.
16. In population data, one sees a good correlation between post-meal glucose and insulin but a poor correlation between *FG* and *FI* (Diwekar-Joshi & Watve, 2020).
17. Although *FG* and *FI* are poorly correlated in prediabetic states, HOMA- β and HOMA-IR have strong positive correlations in population data (Diwekar-Joshi & Watve, 2020).
18. Failure of glucose normalization to reduce the frequency of complications and mortality: Unlike T1DM, in T2DM, tight regulation of plasma glucose has failed to show a reduction in mortality consistently across multiple large-scale clinical trials (Diabetes Prevention Program Research Group, 2015; Ferrannini & DeFronzo, 2015; King et al., 1999; Klein, 2010; Lee et al., 2021; Schwartz & Meinert, 2004; R. Turner et al., 1998; The NICE-SUGAR Study Investigators, 2009, UK Prospective Diabetes Study (UKPDS) Group, 1998). If hyperglycemia is the primary pathology of type 2 diabetes, preventing or correcting it should have reduced the frequency of complications and mortality considerably.
19. Reversal of hyperglycemia by FGF 21 in all models of rodent diabetes: Independent of the cause of hyperglycemia, a single injection of FGF 21 was able to achieve long-term normalization of plasma glucose (Laeger et al., 2017).

While most models intend to explain 1, 2 and 5 of the above, they either fail to explain or do not address the others. Our expectation from a satisfactory model is that it should inherently predict these outcomes or should be compatible with them. If an additional explanation that does not contradict the model accounts for the phenomenon, the model can be said to be compatible. Compatibility with empirical findings cannot be taken as proof or validation of the model, but if a model directly contradicts one or more of the empirical findings, it becomes serious grounds for rejecting the model. Later, when we describe model results, we will use the numbers in the above list in square brackets to indicate that the model accounted for this pattern.

1.2. Peripheral models of glucose homeostasis

There is a rich history of the development of mathematical models of glucose homeostasis and the origin and progression of type 1 and type 2 diabetes (reviewed by Ajmera et al., 2013; Mari et al., 2020). The focus of the field is so much on the peripheral mechanism that the review by Mari et al. (2020) does not even cite the models incorporating the role of the brain. Ajmera et al. (2013) briefly mention the Gouhua et al. (2009) model but do not elaborate on its potential implications. A class of models attempts to capture glucose homeostasis at the systems levels, whereas other models look at individual components such as insulin-dependent glucose uptake, liver glucose production, β cell dysfunction, glucose-stimulated insulin secretion and incretin effects in greater detail. Nevertheless, these models together have not accounted for the majority of the patterns listed above. The central assumption of these models is more or less invariant and revolves around insulin resistance and the failure of insulin response to adequately compensate for it (Mari et al., 2020). Diwekar-Joshi and Watve (2020) claimed that any model with this set of assumptions is not compatible with empirical patterns 3,4,6,9, 16 and 17 of the above. Whether any variation of these models can do so has not been adequately explored. Furthermore, all the peripheral regulation models are CSS models in that the fasting steady state is a consequence of the rate of liver glucose production and a concentration-dependent rate of glucose uptake. In these models, a change in either or both the rates inevitably alters the steady state. This contrasts the TSS models in which alteration in these rates alters the time required to reach a steady state but does not alter the steady-state glucose level (Diwekar-Joshi & Watve, 2020). An attempt to develop a TSS model with only peripheral mechanisms has not been made to the best of our knowledge.

We do not intend to review glucose homeostasis models here. However, we observe from published reviews of glucose homeostasis models (Ajmera et al., 2013; Mari et al., 2020) that most models do not

address the apparently anomalous empirical findings, particularly 3,4,6,9,10,11,12,13 and 15-18 among the ones listed above. A detailed exploration into whether some variations of these models can address the apparently anomalous patterns is beyond the scope of this paper, but we remain open to this possibility.

1.3. Brain-centered models of glucose homeostasis

It is quite well known that a number of neuronal mechanisms in the brain are involved in energy homeostasis. Nevertheless, for some reason, they do not occupy a central stage in the mainstream thinking in T2DM and glucose regulation models. A number of recent publications highlight the role of the brain in different ways (Lam, 2005; Osundiji et al., 2012; Perrin et al., 2004; Watve, 2013; Lundqvist et al., 2019). Peters (2004), Gaohua and Kimura (2009) and Watve (2013) proposed that the primary target of glucose homeostasis is to regulate glucose levels in the brain. Plasma glucose levels are only a means to achieve the required supply of glucose to the brain. Since the transport of glucose to the brain is more restricted, when an adequate supply of glucose to the brain is ensured, it is likely that the supply to other organs is already ensured.

In the Gaohua and Kimura (2009), as well as in the Watve (2013) model, the rate of glucose transport across the BBB is assumed to be an adaptation to hyperglycemia. The finding that glucose transport is reduced to an intermediate level in obese and prediabetic individuals (Büsing et al., 2013; Hwang et al., 2017) suggests that the deficiency in transport precedes hyperglycemia rather than following it. Therefore, it is more likely to be causal than consequential. Glucose deficiency in the brain is known to induce liver glucose production and suppress insulin release through autonomic control (Boland et al., 2017). Sympathetic tone has also been shown to be higher in T2DM (Thackeray et al., 2012). Therefore, glucose deficiency in the brain owing to altered vascular function is likely to be primary, which results in altered plasma glucose dynamics mediated by autonomic inputs. Our model incorporates this possibility.

Impaired vascular function is known to be central to diabetic complications. The classical thinking has been that hyperglycemia causes the types of vasculopathies typical of T2DM. However, it has not been ruled out that vasculopathies are not primary. There is considerable evidence that microvascular alterations precede T2DM and are good predictors of it (Muris et al., 2012; Nguyen et al., 2007; Stehouwer, 2018; Zaleska-Żmijewska et al., 2017). A sedentary lifestyle and deficiency of many specific types of physical activities and behaviours alter the expression of growth factors and endocrine mechanisms involved in angiogenesis (Watve 2013). It has been demonstrated repeatedly that many growth factors and angiogenic factors are responsive to behaviours, physical activity and exercise (Aloe et al., 1994; Cao

et al., 2010; Chodari et al., 2016; Lakshmanan, 1986; Nexø et al., 1984; NEXØ et al., 1981; Tirassa et al., 2003). A deficiency of these behaviours is likely to lead to a primary deficiency of angiogenic mechanisms (Watve, 2013). We consider the possibility that altered vascular function in the brain is the primary reason why glucose transport from blood to the brain is reduced. This creates chronic glucose deficiency in the brain, to which the brain reacts by influencing multiple mechanisms of glucose regulation. The predominant mechanism is autonomic signalling. It is well known that sympathetic and parasympathetic tones are altered in T2DM (Thackeray et al., 2012). We consider the possibility that altered autonomic signalling is causal rather than consequential to diabetes based on studies showing that changes in autonomic function precede T2DM (Carnethon et al., 2003).

The brain glucose uptake is insulin-independent (Gray et al., 2014; Hasselbalch et al., 1999). Nevertheless, insulin has many other functions in the brain and insulin signalling is known to be important in memory, cognition, decision making and behaviour (Kerns, 2001; Shemesh et al., 2012; Strachan, 2003). The brain is rich in insulin receptors, and activation of certain cognitive functions in the brain is a likely cause of increased brain glucose utilization by insulin stimulation (Bingham et al., 2002; Rebelos et al., 2021). We assume, therefore, that the brain has a fundamental requirement for insulin, independent of glucose metabolism and therefore, mechanisms to ensure the required insulin levels in the brain are as critical as ensuring minimum brain-glucose level. This is also ensured by autonomic mechanisms. Autonomic inputs are known to regulate β cell population as well as insulin release from β cells (Thorens, 2015). Therefore, our model also incorporates brain control over insulin production.

Ensuring a minimum supply of glucose as well as insulin to the brain is crucial during fasting when the plasma levels are low. The post-meal levels of glucose and insulin in the plasma are much higher, and at this time, the brain need not actively regulate the plasma levels of both. This can be taken care of by the peripheral mechanisms.

1.4. Objectives of the model

Our attempt is to construct a model whose predicted outcomes match with all or most of the observed phenomena listed above qualitatively. We intend to construct a model in which different hypotheses for hyperglycemia can be used to make differential testable predictions. This approach can allow us to evaluate comparatively which causal factors, individually or in combination, can give us the set of predictions that match the patterns listed above.

Out of the parameters required for the model, only some have empirical estimates available (table 1). In the absence of realistic estimates of all parameters, we do not intend to make a model making quantitative predictions. When a sufficiently large number of parameters can be optimized, it is not difficult to fit the data quantitatively. Therefore, we prefer qualitative predictions over quantitative ones. We test whether the model is able to predict the pattern observed empirically under some set of parameters. The ability to predict a given pattern is not proof of the validity of the model, but the inability to predict an observed phenomenon at any set of parameters in a realistic range is a strong reason to call the model either inadequate or wrong. If an additional consideration compatible with the model is able to explain a pattern not explained by the main model, the model can be called inadequate but not falsified. However, if the model outcome directly contradicts a consistent and reproducible empirical finding, it can be considered falsifying evidence. We emphasize the need to evaluate our model in comparison with classical models on these lines.

2. Methods

2.1. *Assumptions of the model*

A unique assumption of our model based on the analysis by Diwekar-Joshi and Watve(2020) is that the mechanism of regulation of glucose and insulin is different in the steady state and post-meal state. In the steady state, the central mechanisms are more important, whereas, in the post-meal state, mainly the peripheral mechanisms are at work. Insulin-induced glucose uptake and insulin-dependent inhibition of liver glucose production happen only above a threshold glucose and insulin level, respectively. The presence of such thresholds and their context-dependent variability has been known for a long time (Chen et al., 1993; Henquin et al., 2006; Sorensen, 1985). Below the threshold, other mechanisms regulate the levels (Sorensen 1985). We assume in the model that the thresholds are under neuroendocrine control and fine-tuned by the brain. The thresholds found in isolated cell cultures are slightly lower than the normal fasting blood sugar, and it is difficult to estimate thresholds in vivo (Chen et al., 1993; Henquin et al., 2006, 2015). In the presence of autonomic signals, we assume the thresholds to be above the steady-state target levels. In conditions under which the fasting levels need to increase, we assume the thresholds to increase proportionately. This may happen with peripheral or central mechanisms. These assumptions about the threshold make the model a TSS model.

The steady-state glucose is decided by a balance between the basal level of liver glucose production, which is regulated by neuronal mechanisms and insulin-independent glucose uptake by tissues. The steady-state insulin level is decided by the basal rate of glucose independent insulin production, which is regulated by neuronal mechanisms against the insulin degradation rate. Glucose is transported from plasma to the brain by facilitated diffusion proportionate to capillary surface area in the brain and glut-1 expression. Steady-state brain glucose is determined by glucose transport to the brain and utilization by brain tissue. The brain needs a target level of glucose, and the brain ensures it by directly regulating liver glucose production by neuronal mechanisms.

Insulin has cognitive and other functions in the brain (Begg & Woods, 2013; Kern et al., 2001; Rohner-Jeanrenaud & Jeanrenaud, 1983; Shemesh et al., 2012; M W J Strachan, 2005), for which the brain requires a target level of insulin, which it ensures by autonomic regulation of β cell number and basal insulin secretion independent of glucose. To ensure the brain's target level for insulin, a minimum plasma insulin level needs to be maintained. Maintenance of this level is assumed to be independent of glucose-stimulated insulin secretion.

The rate of transport of glucose and insulin from blood to the brain is not constant. Both are affected by the capillary density and blood flow. But they also depend upon specific transport mechanisms. Glucose is transported across the blood-brain barrier mainly through the specific transporter glut-1. The expression of glut-1 in the brain and other tissues is variable and dependent on multiple dietary, endocrine and growth factor-related mechanisms (Boado et al., 1994; Ge et al., 2011; Liu et al., 2018; Schüler et al., 2018). Glucose transport from blood to the brain is diminished in obesity and prediabetes (Hwang et al., 2017). Insulin transport to the brain is also reduced in obesity (Begg, 2015). The ratio of CSF to plasma insulin is inversely proportionate to obesity and insulin resistance (Gray & Barrett, 2018). Moreover, inducing endothelial dysfunction and reducing glucose transport experimentally by endothelial-specific deletion of HIF 1- α resulted in hyperglycemia (Huang et al. 2012). These findings validate our assumptions based on which we incorporate the possibility of diminished glucose and insulin transport to the brain being the primary pathology of T2DM and hyperglycemia only as a consequence.

The model

Since we assume that the steady state and post-meal mechanisms of glucose regulations are not identical, we model and analyze the two states in two phases of the model. The variables and parameters

used in the model and the range of parameters used are in Table 1.

s no	Variables and parameters	meaning	units	Value/range used in simulations
A. Input parameters				
1	K_1	Insulin-independent glucose uptake maximum	mg/dL/min	20-50
2	K_{1m}	Half saturation constant for insulin-independent glucose uptake	mg/dl	50
3	K_2	Maximum insulin-induced suppression of PG, including glucose disposal and suppression of L.	per μ U/mL	0.001 to 0.05
4	K_{2m}	Half saturation constant for insulin-induced suppression of PG	μ U/mL	15
5	K_5	Maximum glucose-dependent insulin secretion	μ U/mL/min	2-20
6	K_{5m}	Half saturation constant for glucose-induced insulin secretion	mg/dL	50
7	K_8	Maximum rate of glucose transport to the brain	Mg/dL/min	3 - 8
8	K_{8m}	Half saturation constant for glucose transport to the brain	mg/dL	50-100
9	K_9	Maximum rate of Insulin transport to the brain	μ U/mL/min	0.6 - 1
10	K_{9m}	Half saturation constant for insulin transport to the brain	μ U/mL	0.3-1
11	K_{10}	Brain glucose utilization rate	unitless	0.08 to 0.12
12	d_1	Insulin degradation rate	unitless	0.1 to 0.2
13	BG_t	Target BG	mg/dL	25
14	BI_t	Target BI	μ U/mL	1-5
15	I_s	Insulin sensitivity as compared to normal, which is assumed 1.	unitless	0-1

s no	Variables and parameters	meaning	units	Value/range used in simulations
16	L_{max}	Maximum capacity of liver glucose production	Mg/dL/min	30
17	K_{4max}	Maximum capacity of glucose-independent insulin secretion	μ U/mL/min	10
B. Derived variables				
18	L	Rate of liver glucose production	mg/dL/min	Eq. 6 or iterative
19	K_4	Rate of glucose-independent insulin secretion	μ U/mL/min	Eq 7 and 8 or iterative
C. Outcome variables				
20	PG	Plasma glucose	Mg/dL	dynamic
21	PI	Plasma insulin	μ U/mL	dynamic
22	PG	Steady-state plasma glucose	mg/dL	Eq. 5
23	PI	Steady-state plasma insulin	μ U/mL	Eq. 7
24	BG	Brain glucose	mg/dL	dynamic
25	BI	Brain insulin concentration	μ U/mL	dynamic
26	PGT	glucose threshold above which GSIS begins	mg/dL	5 to 10 mg/dL above PG
27	PIT	The insulin threshold above which insulin-induced glucose disposal begins	μ U/mL	2-5 μ U/mL above PI

Table 1. All variables and parameters considered in the model.

A. Modeling steady-state glucose

As per the assumption, below a threshold PI , insulin-induced glucose uptake and insulin-induced inhibition of liver glucose production are negligible. Therefore, we write,

1. Plasma Glucose:

$$\frac{dPG}{dt} = \begin{cases} L - \frac{K_1 * PG}{K_{1m} + PG} + Gt & (PI < PIT) \\ L - \frac{K_1 * PG}{K_{1m} + PG} + Gt - \left(I_s * \frac{K_2 * PI}{K_{2m} + PI} \right) * PG, & (PI > PIT) \end{cases} \quad (\text{Eq. 1})$$

2. Plasma Insulin:

$$\frac{dPI}{dt} = \begin{cases} K_4 - (d1 * PI), & (PG < PGT) \\ K_4 - d1 * PI + \frac{K_5 * PG}{K_{5m} + PG} * (PG - PGT), & (PG > PGT) \end{cases} \quad (\text{Eq. 2})$$

3. Brain glucose:

$$\frac{dBG}{dt} = \frac{K_8 * (PG - BG)}{K_{8m} + (PG - BG)} - K_{10} * BG \quad (\text{Eq. 3})$$

Since the brain forms only about 3 % of total body mass, we assume plasma glucose diffused to the brain is a negligible fraction of total plasma glucose. Therefore, that term is not included in the plasma glucose dynamics. Similarly, insulin diffusion to the brain is not represented in the plasma insulin dynamics. Nevertheless, the rate of plasma to brain diffusion is crucial in determining the brain glucose and insulin dynamics.

4. Brain insulin:

$$\frac{dBI}{dt} = \frac{K_9 * (PI - BI)}{K_{9m} + (PI - BI)} - d_1 * BI \quad (\text{Eq. 4})$$

At steady state (SS), all differential terms become zero, and steady-state levels can be calculated using equilibrium solutions.

As per the assumption of the model, the brain needs a certain level of glucose, and that is the target of homeostasis BG_t . In order to ensure BG_t at given K_8 , K_{10} and K_{8m} , the SS plasma glucose PG needs to be

$$\underline{PG} = \frac{BG_t * K_{10} * K_{8m}}{K_8 - (BG_t * K_{10})} + BG_t \quad (\text{Eq. 5})$$

We assume that the brain ensures this plasma glucose level by regulating liver glucose production L . To maintain the desired plasma glucose level at a steady state, the liver glucose production should be:

$$L = \frac{K_1 * PG}{K_{1m} + PG} \quad (\text{Eq. 6})$$

The brain can either ensure this by sending a calculated signal to the liver through the autonomic system. Alternatively, this can be ensured by the brain by increasing sympathetic inputs when $BG < BGt$ and parasympathetic when it is above target (Antuna-Puente et al., 2009; D'Alessio et al., 2001; Kiba, 2004). The required L can be achieved iteratively by $L_{(t+1)} = L_{(t)} + K_s \cdot (BGt - BG)$

Similarly, to ensure required brain insulin levels, plasma insulin should be

$$\underline{PI} = \frac{d_1 * BI_t * K_{9m}}{K_9 - (d_1 * BI_t)} + BI_t \quad (\text{Eq. 7})$$

To ensure this much plasma insulin level, K_4 should be

$$K_4 = d_1 \cdot \underline{PI} \quad (\text{Eq. 8})$$

Similar to glucose, the brain can ensure the target level of insulin in the brain by neuronally modulating K_4 in a calculated or iterative manner. Specific autonomic inputs are known to regulate β cell number as well as insulin release from β cells (Begg & Woods, 2013; Boland et al., 2017; Kiba, 2004).

We also assume that both L and K_4 have a fixed upper limit as L_{max} and K_{4max} when the maximum capacity of the liver and pancreas is reached. L and K_4 cannot exceed this limit even if neuronal inputs become more intense. This happens when K_8 declines below a threshold such that,

$$K_8 < \frac{K_1 - L_{max} (BGt * K_{10} * K_{8m})}{L_{max} * K_{1m} - BGt (K_1 - L_{max})} - (BGt * K_{10}) \quad (\text{Eq. 9})$$

There is a potential conflict here. Sympathetic tone is known to increase L (Nelles et al., 1996; Nonogaki, 2000), whereas parasympathetic signal is required for proliferation of β cells. Simultaneously, a sympathetic signal is known to inhibit insulin release from β cells (Gilon & Henquin, 2001; Miller et al., 1976). If the brain is deficient in glucose as well as insulin, both sympathetic and parasympathetic tones will be simultaneously higher (Watve et al., 2014). This is incorporated into the model by updating K_4 iteratively according to both BG and BI levels simultaneously,

$$K_{4(t+1)} = K_{4(t)} + K_p (BI_t - BI) - K_s (BGt - BG) \quad (\text{Eq. 10})$$

By this consideration, if sympathetic stimulation of liver glucose production is adequate to restore required BG , $BGt - BG$ will tend to zero, and there will be no interference in insulin release by β cells. However, in case the rise in liver glucose production is inadequate to ensure required BG , K_4 will be affected, which will apparently influence β cell function.

B. Simulating glucose tolerance curve

While for the steady state, equilibrium solutions can be algebraically derived, the post-glucose load curve and its properties can only be obtained by simulations. Simulations were run using the same set of equations and giving a positive ephemeral G_t to simulate food intake.

In all the simulations used, insulin resistance can be simulated by altering I_s , β cell dysfunction by reducing K_4 and/or K_5 and vascular defect slowing down the transport of glucose and insulin to the brain and other organs by altering K_8 , K_9 and K_1 . Mental stress is assumed to increase K_{10} . By differentially altering these parameters, the model can separately and collectively examine the effects of insulin resistance, β cell dysfunction, reduced rates of diffusion across BBB and stress on the glucose tolerance curve.

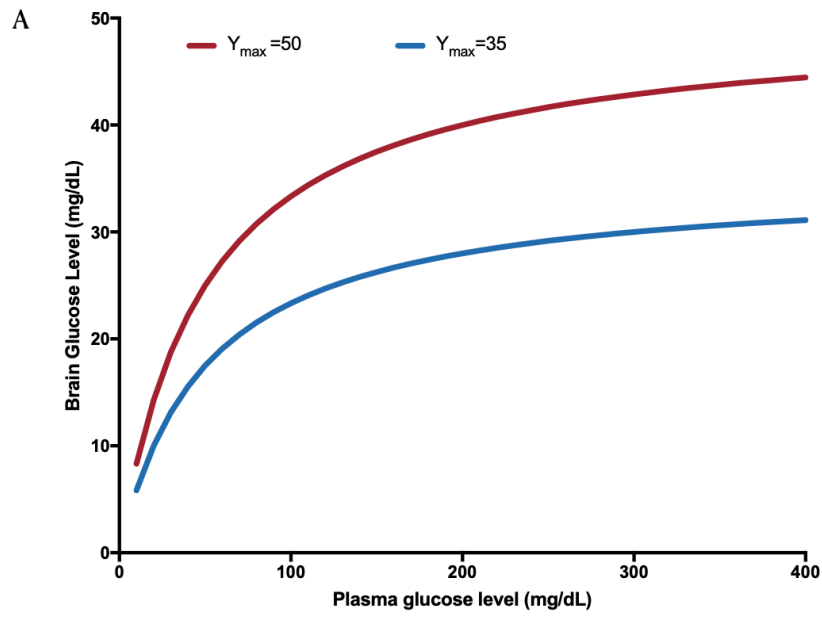
T2DM- causal analysis: We ask the question of which minimal set of changes can give rise to a stable increase in fasting glucose, changes in the glucose tolerance curve characteristic of type 2 diabetes, and other patterns listed above. The putative causal factors are examined individually and in combination. The factors include insulin resistance (Decreased I_s), subnormal β cell response (Reduced K_4 and/or K_5), reduced insulin-independent glucose uptake (decrease in K_1), reduced blood-to-brain transmission of glucose (K_8) and insulin (K_9) and stress-related increase in brain glucose consumption (K_{10}). Subnormal or defective vasculature is expected to decrease K_1 , K_8 and K_9 proportionately; however, the decrease in the three parameters may not be proportionate if the vasculature in different parts of the body is differentially affected. Also, glucose transporters and their expressions can alter in a tissue-specific manner. Therefore, we allow proportionate as well as differential decrease in the three parameters.

Results

A. Steady-state solutions: We observed that the steady-state solutions and the autonomic iteration simulations match well in the end result except when the limits of L and K_4 are reached. However, it took a long time to reach the desired level by iterative approach, particularly when the desired level was substantially different from the starting level. In real life, major changes in vascular function or glucose transporter levels reflected in K_8 , K_9 , and K_1 happen gradually. Therefore, the desired level can be attained by autonomic fine-tuning over time. Since, in the iterative simulations, a long time was required to reach SS, we used the steady-state solutions for quicker results.

It can be seen that the steady-state levels of PG in the model is a stable, steady state since substituting $PG < \underline{PG}$ leads to a positive value and $PG > \underline{PG}$ leads to a negative value of $\frac{dPG}{dt}$. The same applies to plasma insulin, brain glucose and brain insulin. This ensures a stable, steady state of glucose-insulin in the plasma as well as in the brain on fasting [1,2]. From equations 5,6, and 8, we see that FG does not change by altering I_s or FI . This is compatible with the empirical findings that insulin receptor knockouts and insulin suppression experiments fail to increase fasting plasma glucose [9]. This result is unique to our model and is due to segregating fasting and post-meal glucose regulation mechanisms by using thresholds. This is the only explanation offered so far for patterns [9], [16] and [17].

The steady-state solution of our model shows that FG can increase as a result of an increase in K_{I0} or a decrease in K_g . That is, if the glucose consumption in the brain increases and/or the rate of glucose transport from blood to the brain decreases. Both the effects are interdependent, and the shape of the glucose response is decided by the interaction between K_g and K_{I0} . Increased K_{I0} increases FG marginally and almost linearly when K_g is large. When K_g decreases, even a marginal rise in K_{I0} can induce a disproportionately greater rise in FG (fig 1). This means that stress-induced hyperglycemia is unlikely to be seen in healthy individuals, while it is more likely in individuals with reduced vascular transport [7].



B Effect of brain glucose transport and utilization on fasting glucose levels

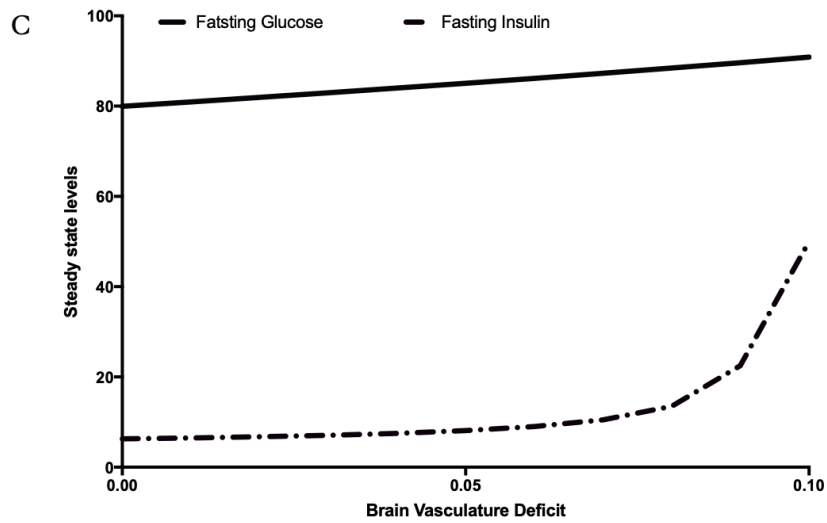
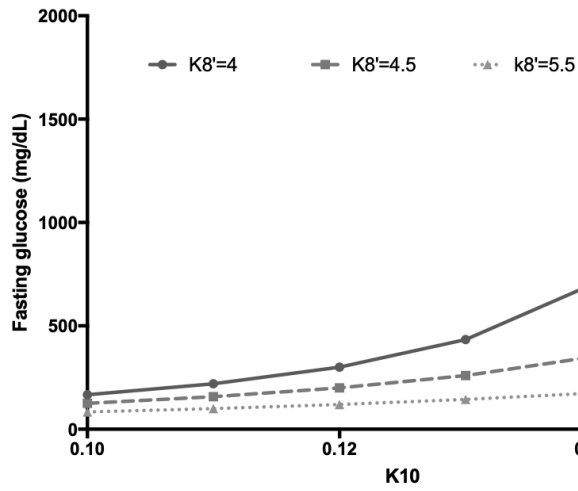


Figure 1. The same input different output phenomenon:

A. A conceptual diagram with arbitrary units: A saturation relationship in glucose and insulin transport described by a Michaelis Menten type of equation has important consequences that can account for many phenomena observed in prediabetic and diabetic stages. For example, here, for achieving an increase in Y by 6 units with a higher Y_{max} , X needs to increase only by 6 units, but at a lower Y_{max} for the same target increase in Y , 25 units of increment in X is needed. This non-linearity explains many phenomena, including prediabetic hyperinsulinemia and stress-induced diabetes in our model of glucose homeostasis.

B. A simulation using the steady state model: It can be seen that as K_8 decreases, for the same change in brain requirement K_{10} , a non-linear escalated increase in plasma glucose is required.

C. A simulation result assuming a correlated decrease in K_8 and K_9 . It is possible that while glucose shows a marginal increase, insulin increases substantially, since the parameters of glucose and insulin transport curves are different. This is a potential explanation for the hyperinsulinemic normoglycemic state.

The origin of the hyperinsulinemic normoglycemic condition can be explained by the difference in the parameters of the saturation curves of transport dynamics of glucose and insulin. If the insulin diffusion is assumed to be nearer to saturation and glucose diffusion is sufficiently away from saturation, at the same level of vascular function deficiency, insulin will increase disproportionately more than glucose (Figure 1). This is a possible cause of hyperinsulinemic normoglycemic state [3] and the reason why hyperinsulinemia precedes hyperglycemia [4], which requires neither insulin resistance nor compensatory hyperinsulinemic response. When this happens, both HOMA-IR and HOMA β increase, although there is no change in true insulin resistance and compensatory insulin response. This gives a false impression of insulin resistance as clinically defined.

Further, as the transport saturation constant K_8 and K_9 continue to decrease proportionately, FG increases monotonically, but FI shows a non-monotonic curve in which FI increases with a moderate decrease in transport rates but decreases after a threshold decrease in transport rates. This non-monotonicity is predicted by the iterative autonomic inputs model. When the required L approaches or exceeds L_{max} , the steady state BG remains smaller than BGt . The resultant increase in the sympathetic signal inhibits insulin release from β cells. This leads to reduced insulin secretion, and insulin levels drop substantially. Thus, without bringing in additional factors, the model explains the early phase rise in fasting insulin as well as the later phase decline in the course of T2DM [4] (Figure 2).

Effect of decrease in glucose and insulin transport to brain

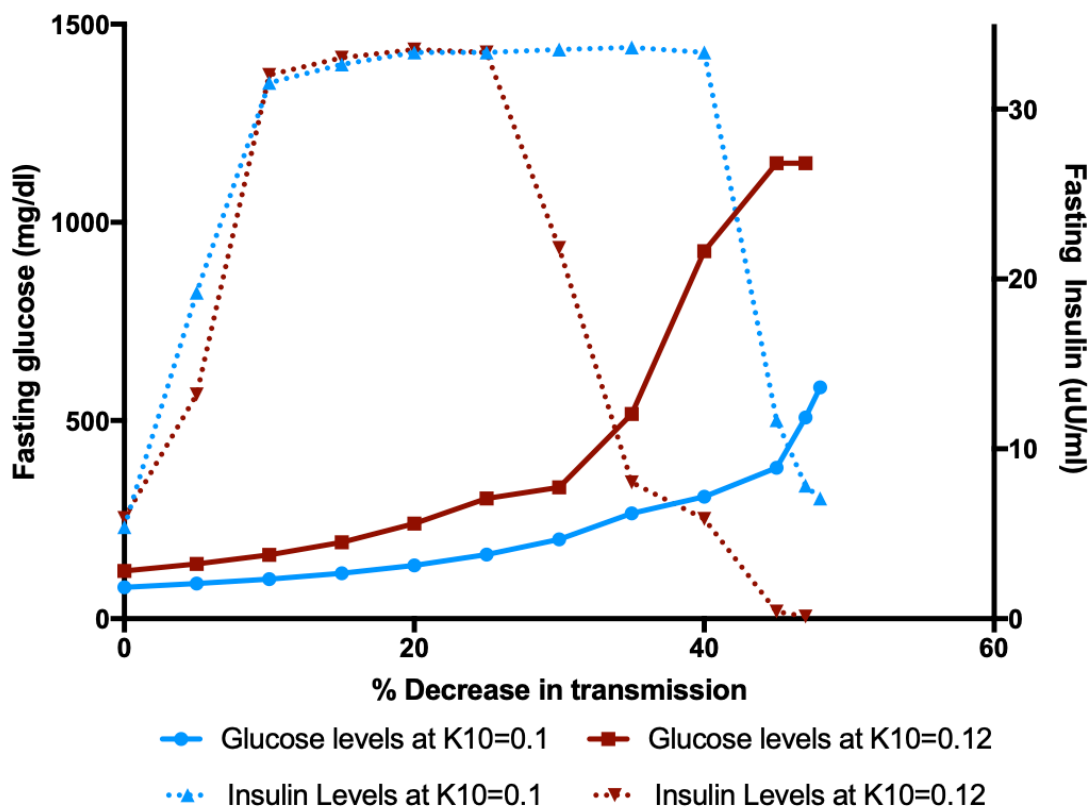


Figure 2. Effect of correlated decrease in K_8 and K_9 on fasting plasma glucose and insulin. Note that for a small to moderate decrease, FI increases rapidly with marginal change in FG. However, after a threshold decrease in the transport rates, FI declines sharply, whereas FG increases rapidly. This pattern matches with the course of clinical T2DM without involving insulin resistance, compensatory hyperinsulinemia and β cell exhaustion. Simulation-specific other parameters were $K_{1m}=50$, $K_1=30$, $K_{2m}=15$, $K_2=0.01$, $K_{5m}=0.01$, $K_5=0.5$, $d_1=0.15$, $I_s=1$, $BGt=25$, $Blf=5$, $K_{8m}=80$, $K_8=5$, $K_{9m}=0.3$, $K_9=0.8$, $K_{10}=0.1$ (Blue line) and 0.12 (Red line).

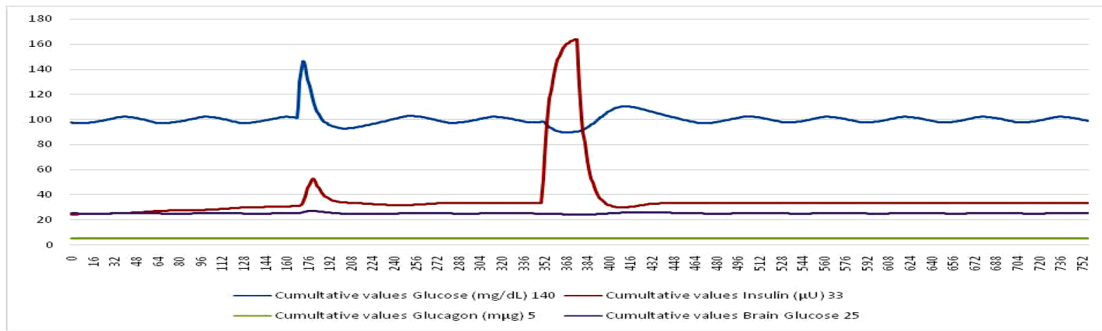
This decline in the insulin response does not require β cell dysfunction as a causal mechanism, but there are more complex possible effects on β cells. Simultaneous activation of sympathetic and parasympathetic inputs to β cells is implicated in β cell amyloidogenesis (Watve et al., 2014). Parasympathetic stimulation is known to increase β cell number. However, sympathetic signalling suppresses insulin release resulting in increased retention time of insulin along with amylin which, beyond threshold retardation, may result in spontaneous polymerization of amyloid protein leading to poisoning of β cells and amyloidogenesis (Watve et al., 2014). This is an alternative causal interpretation

of β cell dysfunction and decline in its population. This mechanism has a built-in negative feedback loop, giving rise to a steady-state β cell population. This result is compatible with the finding that the β cell population remains subnormal lifelong [11,12]. This is in contrast with the dynamics expected by classical thinking in which β cells are destroyed by gluco-lipotoxicity or oxidative stress. This mechanism has a built-in positive feedback cycle. As a part of the β cell population is destroyed, insulin secretion is decreased, which would increase glucose, further accelerating gluco-lipotoxicity and oxidative stress and thereby β cell loss. Such a positive feedback vicious cycle can only stop with the complete destruction of the β cell population. This prediction of the classical model does not match the finding of sustained presence of subnormal β cell population in T2DM.

By the classical model, prolonged sustained exercise in the fasting state should result in lower plasma glucose. However, an experimental increase in glucose uptake resulting from physical activity during fasting does not necessarily result in a decrease in FG . This is mainly because as FG starts decreasing, BG decreases consequently. BG being lower than BG_t induces a sympathetic-mediated increase in L , and the change in FG by physical activity is more or less compensated. This may happen through the agency of glucagon as well since a strong link between autonomic signals and glucagon secretion is known. Therefore, at times, plasma glucose may actually increase after intensive exercise. Further, if exercise involves heightened activation of cerebellar mechanisms of coordination, K_{I0} may also increase, resulting in higher rather than lower FG in response to exercise [8].

A high dose of exogenous insulin results in increased plasma glucose after a time lag, which is known as the Somogyi phenomenon. The phenomenon is conditional and not seen in every diabetic. It is said to involve the counter-regulatory response to facing central hypoglycemia. However, often, this response is seen without peripheral hypoglycemia. This is best explained by reduced K_{δ} , which gives rise to a decreased BG/FG ratio. With smaller K_{δ} , at apparently normal or increased plasma glucose, brain glucose can still be lower than the target, which gives a sympathetic signal to increase L . Simulations using the autonomic iteration model show this phenomenon quite well at low K_{δ} . At the same level of insulin infusion, at lower K_{δ} there is a more intense hyperglycemic response (Figure 3) [14]. A model without accommodating changes in K_{δ} does not predict the Somogyi phenomenon without an obvious hypoglycemic state.

At transportation rate 90%



At transportation rate 70%

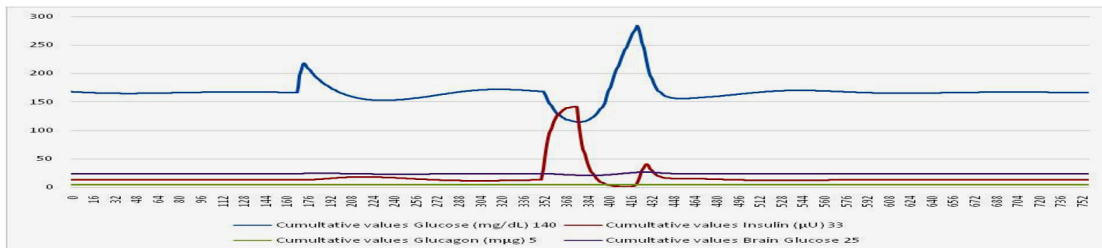


Figure 3: Effect of high-dose insulin on peripheral glucose under two rates of glucose and insulin transport across the blood-brain barrier (Correlated decrease in K_8 and K_9). A paradoxical rise in blood sugar following insulin administration is more prominent when the transport rate is substantially lower than normal. Other parameters ($K_{1m}=50$, $K_1=30$, $K_{2m}=15$, $K_2=0.08$, $K_{5m}=0.01$, $K_5=15$, $d_1=0.15$, $I_s=1$, $BG_t=25$, $Bl_t=4.5$, $K_{8m}=80$, $K_8=5$, $K_{9m}=0.3$, $K_9=0.8$, $K_{10}=0.1$)

The response is restricted to a narrow set of conditions. For intense hyperglycemic response to insulin administration, it is necessary that insulin sensitivity is good, BG is close to BG_t before insulin transfusion, and K_8 is subnormal.

Potentially, one can visualize two distinct possible classes of reasons why blood sugar increases in response to brain injury. In the first, there is some impairment in the glucose regulation mechanism. In the second, the requirement for glucose is increased during the wound healing process, and hyperglycemia is a mechanism of the body to meet the demand. It is known that infections such as meningitis, stroke or haemorrhage lead to transient hyperglycemia. Such hyperglycemia is often accompanied by lower BG levels (Schut et al., 2009; van Veen et al., 2016)[15]. In such cases, hypoglycemic treatments can be counterproductive and result in a delayed or derailed repair process. This is a likely

reason why, in patients under intensive care, strict regulation of plasma glucose increases mortality instead of the expected decrease (The NICE-SUGAR Study Investigators, 2009).

When hyperglycemia is a process of meeting increased glucose demand or compensating subnormal transport, the removal of plasma glucose by any means is expected to increase L . This is observed to happen when SGLT2 inhibitors decrease the urinary threshold and drive out plasma glucose. If increasing L is not sufficient to restore the required glucose level, there is a shift to ketogenesis since the brain can use keto acids as an alternative source of energy. Therefore, increased L with or without increased ketogenesis is expected by our model following SGLT2 inhibitors [13].

B. Glucose tolerance curve: Unlike the steady-state predictions, the patterns of the post-feeding glucose curve by our model are not qualitatively different from classical models. The area under the curve, the height of the peak, the time required to return to a steady state and the time difference between glucose and insulin peaks are increased by decreased I_s , K_5 , or K_8 individually or in combination. Decrease in I_s or K_5 does not increase FG but changes the shape of the glucose tolerance curve. Decreased K_8 may alter both simultaneously. The altered curve shows the three typical features, namely a taller peak, delayed return to a steady state and a longer gap between glucose peak and insulin peak [5]. This result is not unique to our model, and classical models also show the three features. The classical model results in simultaneous and proportionate alterations in the fasting as well as post-meal glucose and, therefore, fails to explain the NFG-IGT state. In our model, decreasing I_s or K_1 without a change in K_8 results in an NFG-IGT state [6].

C. Population simulations: For the steady state as well as post-glucose load dynamics, we give population distributions to K_1 , K_5 , K_8 , K_9 , I_s and also incorporate normally distributed error in glucose and insulin measurements in fasting and post-meal sampling. We also incorporate correlated changes in K_1 , K_8 and K_9 which are expected as a result of hypo-vascularization in the brain. These simulations are run to observe whether we get the anomalous correlations in fasting versus post-meal state and in the HOMA indices as observed empirically (Chawla et al., 2018; Diwekar-Joshi & Watve, 2020).

By classical models, the regression correlation parameters of the glucose-insulin relationship are not different in the fasting state versus post-glucose load, although the range of variables is different, as shown previously by Diwekar-Joshi and Watve (2020). Also, if we assume HOMA-IR to faithfully reflect insulin resistance and HOMA β to faithfully represent β cell response, then there is no reason why the two indices should be correlated.

The assumption behind our model that there are different mechanisms at work under fasting versus post-glucose load conditions is necessary to explain the large difference in the regression correlation parameters in fasting versus post-meal levels. If the same set of mechanisms in the fasting and post-meal conditions are operational, whatever the model used, it is imperative that fasting correlation regression parameters are stronger or comparable to post-meal parameters. Simulations with our model are able to give poor *FG-FI* correlation along with strong post-meal glucose insulin correlation under multiple conditions [16] (Figure 4). When the variance in K_8 and K_9 is small but that in K_I , K_5 , Gt and I_5 individually or in combination is large, the fasting correlations are weak and post-meal correlations strong; the post-meal glucose-insulin regression slope is substantially greater than *FG-FI* slope. Also, whenever the *FG-FI* correlation is weak, the indices HOMA-IR and HOMA β are strongly correlated, similar to the epidemiological data [17]. The difference between fasting and post-meal regression correlation patterns is not predicted by the classical models and is unique to our model, which assumes a different set of regulatory mechanisms in the fasting and post-meal state.

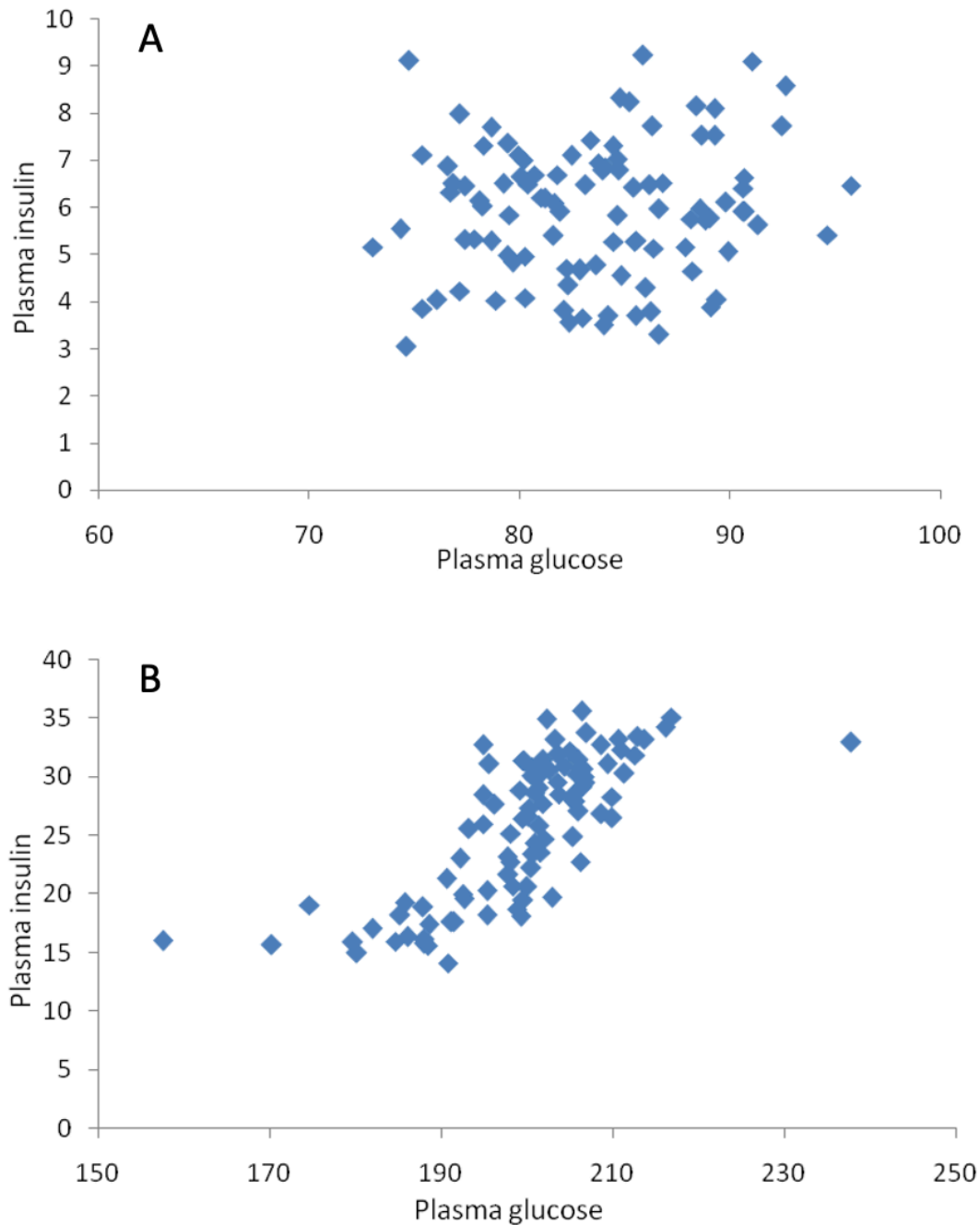


Figure 4. Plasma glucose and insulin correlation in the fasting steady state (A) and post-meal (B) in simulations. The empirical finding that there is a strong positive correlation in the post-meal data but poor correlation in fasting steady state was possible under a variety of conditions in our model. Depicted here are the simulation results (post-meal $R^2=0.57$, steady state $R^2=0.014$) in which only K_1 was given a wider population distribution. (mean (S.D.) $K_1 = 35(7)$, $K_5 = 10(0.00001)$, $K_8 = 5(0.000005)$, and $K_9 = 0.8(0.000008)$). Other parameters ($K_{1m} = 50$, $K_{2m} = 15$, $K_2 = 0.05$, $d_1 = 0.15$, $I_s = 1$, $BGt = 25$, $BI = 4.5$, $K_{8m} = 80$, $K_{10} = 0.1$).

D. Effect of glucose normalization on arresting diabetic complications and mortality: By classical thinking, chronic hyperglycemia is responsible for diabetic complications and preventing hyperglycemia should arrest complications. In contrast, the thought behind our model is that vascular problems are primary, which alter the rate of glucose-insulin transport to the brain, and hyperglycemia is an offshoot symptom that may not be causal to diabetic complications. Diabetic complications can arise directly from the vasculopathy. Therefore, controlling glucose may not have any effect on diabetic complications [18]. On the other hand, forcefully reducing plasma sugar without addressing vascular problems can create more severe glucose deficiency in the brain and other organs, thereby turning counterproductive. Because of the saturating dynamics of transport, a curvilinear relationship is expected between plasma glucose and brain glucose in such a way that a moderate reduction in hyperglycemia will change brain glucose availability marginally, whereas tight glucose regulation can have a disproportionately larger effect (Figure 5). Therefore, tight glucose regulation may increase mortality and other adverse outcomes. This prediction is compatible with some of the tight versus moderate control clinical trials, including ACCORD, NICE sugar trial and UGDP [18].

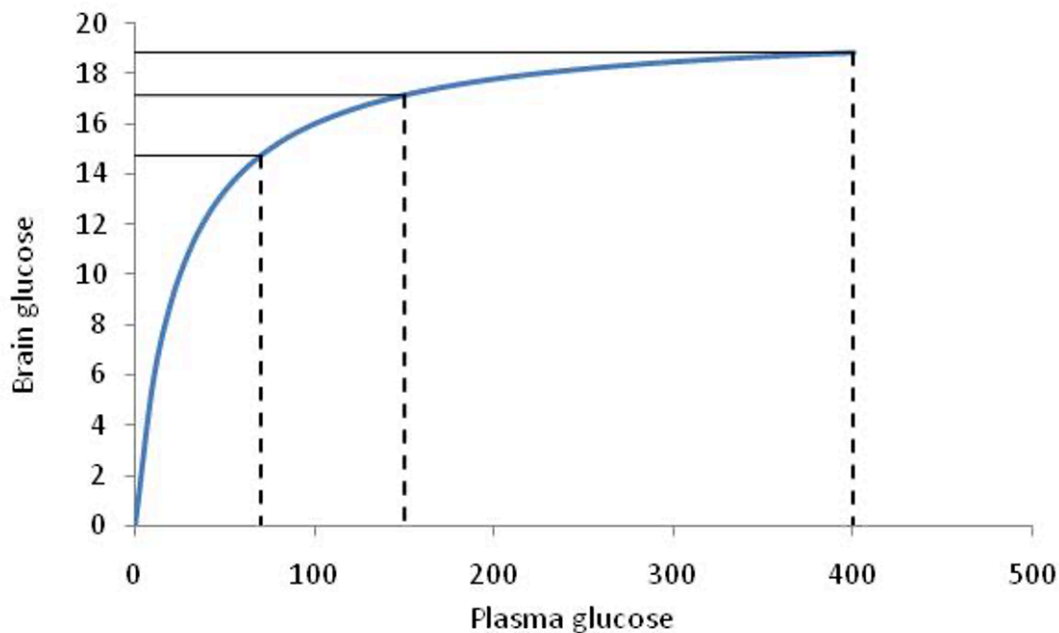


Figure 5. Effect of glucose lowering on brain glucose availability. For example, a reduction in FG from 400 mg/dl to 150 mg/dl corresponds to a decrease in BG by 1.68 mg/dl, but further reduction from 150 to 70 mg/dl reduces BG by 2.41 mg/dl. Therefore, moderate sugar control may not affect brain glucose supply drastically, but tight sugar control is expected to affect it more seriously.

Discussion

The main inference from our model, stated most conservatively, is that a brain-centred model can potentially explain most of the anomalies faced by peripheral models and, therefore, needs greater attention (Figure 6). If supported well, by exploring its testable predictions suggested below and possibly more, it has the potential to bring in a radical change in the fundamental view as well as the clinical practice of T2DM.

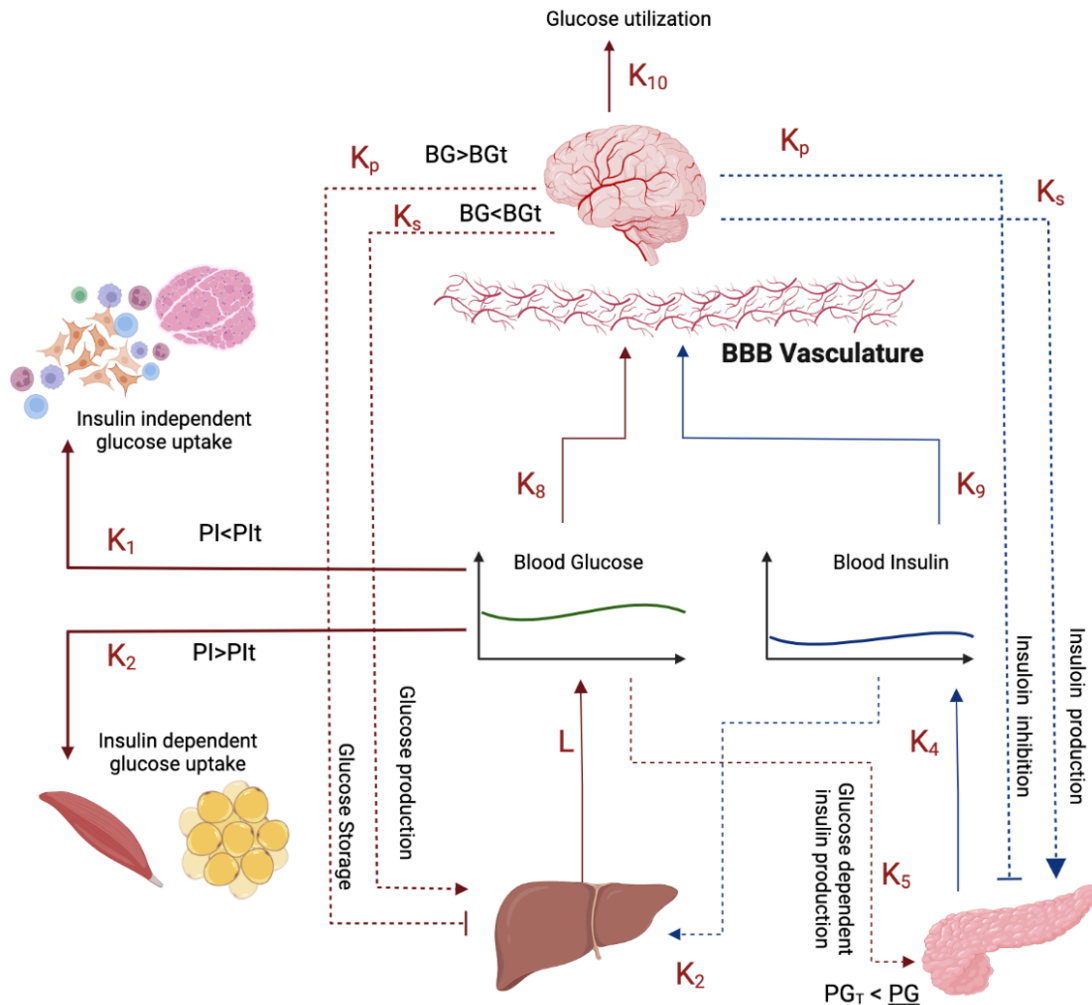


Figure 6. Effect of changes in vasculature in the brain barrier. The model predicts that glucose and insulin transportation to the brain has a major role in the development of diabetic symptoms compared to other peripheral changes. The blood-brain barrier vasculature, hence, may hold the key to understanding the shift from normal to diabetic condition. (created using BioRender)

Testability of assumptions and additional predictions:

The assumption that the thresholds *P_{GT}* and *P_{IT}* can be modified by autonomous signalling needs to be tested empirically. Although, currently, the thresholds are known to be flexible, information about the conditions and mechanisms of change is poorly known. Our assumption is that the parameters of the saturation equation for glucose and insulin transport to the brain are different and, under normal conditions, insulin transport is closer to saturation than glucose transport can be tested with carefully worked out kinetics of the two transport mechanisms.

The assumption of our model that reduced transport of glucose and insulin to the brain is the primary pathology of T2DM leading secondarily to hyperglycemia makes more predictions that can be tested experimentally or epidemiologically. Experimentally, specifically blocking glut1 receptors in the brain should lead to hyperglycemia. Conversely, the infusion of glucose directly into the brain should reduce peripheral hyperglycemia in the short run. This is already suggested by some experiments (Ono et al., 1983; Osundiji et al., 2012). It is also demonstrated that inducing primary endothelial dysfunction and reduced glucose transport to the brain by endothelial deletion of hypoxia-inducible factor HIF-1 α results in hyperglycemia (Huang et al., 2012). More careful research in this direction to reveal the cause-effect relationship between vascular defects, brain glucose levels, and plasma glucose levels will be enlightening. Epidemiologically, hypoglycemia is shown to associate with dementia and other neuronal problems (Lipska & Montori, 2013; Meneilly & Tessier, 2016; Rhee, 2017; Yaffe, 2013), tight glycemic control led to higher mortality as compared to moderate control in many of the clinical trials (Klein, 2010; Schwartz & Meinert, 2004; The NICE-SUGAR Study Investigators, 2009) which demands investigations into the causal pathways. The question of whether tight glycemic control leads to subtle neuronal changes in the long run, as expected by our model, needs careful investigation. The difference between fasting and post-meal regression correlation parameters between glucose and insulin is an important epidemiological line of evidence we have used. Chawla et al. (2017) and Diwekar-Joshi and Watve (2020) showed this pattern across four different data sets. How generalized the pattern is needs to be tested in multiple population studies.

On the modelling front, it is necessary to undertake a comparative evaluation of the different models with respect to the battery of predictions that we listed here. Perhaps a few more predictions may be added. However, at present, many of the models and their possible modifications are not explored sufficiently to see whether they can explain the currently unexplained patterns under certain sets of conditions. A model prediction matrix would be an appropriate approach for such a comparative

evaluation, but we may have to wait till all alternative models are explored sufficiently elaborately on which of the empirical patterns they predict, which ones they are compatible with and which ones they contradict. We have shown here that the brain-centred model predicts or is compatible with all the patterns listed in the introduction and does not contradict any.

Possible causes of T2DM:

The classically believed causal factors, namely insulin resistance and β cell dysfunction, are not compatible with many of the empirical findings, as shown by Diwekar-Joshi and Watve (2020). In our model, changes in insulin resistance and β cell dysfunction were neither necessary nor sufficient to account for all the patterns. Nevertheless, they were helpful in accounting for the altered glucose tolerance curve, although other factors could also account for it independent of insulin resistance. Incorporating insulin resistance in our model and assuming it to work only in the post-feeding state, patterns 1,2,5,6,9,16 and 17 could be explained but not others. In short, our model does not rule out insulin resistance as a phenomenon but implies that it may not be central to T2DM. Primary vasculature impairment reducing glucose and insulin transport in a mutually correlated or uncorrelated manner could explain all patterns and, therefore, makes the most parsimonious causal hypothesis. Particularly, assuming that altered vascular function affects K_1 early, followed by K_8 and K_9 , is sufficient to explain all the patterns without alteration in I_s or any other factor. The apparent β cell dysfunction is an inevitable effect of a higher degree of vascular dysfunction and altered autonomic signals and, therefore, may not be needed as an independent causal factor.

Being open to alternative possibilities is an important virtue of science, and it is particularly important with the limited clinical success of prevalent thinking along with mounting anomalous findings. Prevention of T2DM on a global scale has largely failed, and treatment has limited and inconsistent success in arresting mortality and morbidities associated with T2DM (Brown et al., 2004; DeFronzo, 2010; Rosengren et al., 2008; Lee et al., 2021). Therefore, exploring alternative possible interpretations is a need of the time.

Triggered by multiple anomalies in the theory of glucose homeostasis and the origins of diabetic hyperglycemia, we have articulated here an alternative paradigm which potentially resolves in a logically and mathematically consistent manner many of the anomalous findings. Being mathematically and logically sound and compatible with evidence is not sufficient proof of a theory but certainly reflects its potential to develop into a new alternative paradigm. For a large field such as T2DM, multiple efforts would be needed to evaluate competing paradigms. We have suggested a few more testable predictions

that can help in this task. There can be more possible ways of testing them, which should come to light and be used to reach robust conclusions which have the potential to change the clinical course of prevention as well as treatment of an important global health problem.

If our proposed causal inference that vascular dysfunction is primary to T2DM is necessary and might even be sufficient to lead to all the observed symptoms and patterns is supported by more careful investigations, it explains the failure of glucose normalizing treatment in arresting diabetic complications. Simultaneously, it suggests alternative lines of treatments which should focus on normalizing vascular and neuronal function rather than focusing on glucose normalization. The deficiencies of stimuli normally required for growth factors and other angiogenic and neuroprotective factors can be forecasted as the best bet for the new approach. However, rigorous efforts are needed to strengthen the evidence base for selecting the right one amongst the alternative paradigms.

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